







COVID-Transformer: Interpretable COVID-19 Detection using Vision Transformer for Healthcare

Debaditya Shome ¹, T.Kar ¹, Sachi Nandan Mohanty¹, Prayag Tiwari², *Khan Muhammad³, Abdullah Altameem⁴, Yazhou Zhang⁵ and *Abdul Khader Jilani Saudagar⁴

¹ School of Electronics engineering, KIIT University, Odisha, India; 1804372@kiit.ac.in (D.S.); tkarfet@kiit.ac.in (T.K.); sachinandan09@gmail.com (S.M.)

² Department of Computer Science, Aalto University, Espoo, Finland; prayag.tiwari@aalto.fi

³ Visual Analytics for Knowledge Laboratory (VIS2KNOW Lab), Department of Software, Sejong University, Seoul 143-747, South Korea; khan.muhammad@ieee.org

⁴ Information Systems Department, College of Computer and Information Sciences, Imam Mohammad Ibn Saud Islamic University (IMSIU), Riyadh, Saudi Arabia; altameem@imamu.edu.sa; aksaudagar@imamu.edu.sa

⁵ Software Engineering College, Zhengzhou University of Light Industry, Zhengzhou, China; yzzhang@zzuli.edu.cn

* Correspondence: khan.muhammad@ieee.org (K.M.); aksaudagar@imamu.edu.sa (AKJ.S)

Abstract: In the recent pandemic, accurate and rapid testing of patients remained a critical task in the diagnosis and control of COVID-19 disease spread in the healthcare industry. Because of the sudden increase in cases, most countries have faced scarcity and a low rate of testing. Chest x-rays have been shown in the literature to be a potential source of testing for COVID-19 patients, but manually checking x-ray reports is time-consuming and error-prone. Considering these limitations and the advancements in data science, we proposed a Vision Transformer based deep learning pipeline for COVID-19 detection from chest x-ray based imaging. Due to the lack of large data sets, we collected data from three open-source data sets of chest x-ray images and aggregated them to form a 30K image data set, which is the largest publicly available collection of chest x-ray images in this domain to our knowledge. Our proposed transformer model effectively differentiates COVID-19 from normal chest x-rays with an accuracy of 98% along with an AUC score of 99% in the binary classification task. It distinguishes COVID-19, normal, and pneumonia patient's x-rays with an accuracy of 92% and AUC score of 98% in the Multi-class classification task. For evaluation on our data set, we fine-tuned some of the widely used models in literature namely EfficientNetB0, InceptionV3, Resnet50, MobileNetV3, Xception, and DenseNet-121 as baselines. Our proposed transformer model outperformed them in terms of all metrics. In addition, a Grad-CAM based visualization is created which makes our approach interpretable by radiologists and can be used to monitor the progression of the disease in the affected lungs, assisting healthcare.

Keywords: Vision Transformer; COVID-19; Deep learning; Data science; Healthcare; Interpretability; Transfer Learning; Grad-CAM

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1. Introduction

As of June 2021, there have been 173 million COVID-19 cases worldwide, with new cases rapidly increasing at an alarming rate and showing no signs of abating [1]. If COVID-19 infection is not detected early enough, it can induce a flu-like sickness that can proceed to acute respiratory distress syndrome (ARDS), which can be deadly [2–8]. Due to limited resources and the amount of data accessible to the scientific community, early diagnosis of COVID-19 remains a tough challenge despite recent worldwide research efforts in healthcare [9]. RT-PCR has been the standard and approved diagnostic approach for COVID-19, however it has a number of drawbacks. It is costly, risky to medical staff, and there are just a few diagnostic test kits accessible. Medical imaging

31 techniques such as x-ray and CT-based screening, on the other hand, are relatively
32 safe, faster, and more widely available. X-ray imaging has been frequently utilized for
33 COVID-19 screening in comparison to CT imaging since it takes less imaging time, is
34 less expensive, and x-ray scanners are commonly available even in remote regions [10].
35 Because of the complicated morphological patterns of lung involvement, which can
36 fluctuate in degree and appearance over time, the accuracy of a COVID-19 infection
37 diagnosis using chest imaging is strongly reliant on radiological proficiency. The scarcity
38 of competent radiologists, particularly in developing countries, affects the reliability of
39 sophisticated chest examination interpretation. In a study by Cozzi et al. [11], it was
40 found that chest x-ray imaging achieved a balanced real-world diagnostic performance
41 with accuracy in the range of 76% to 86%, and 89% sensitivity. They showed that the
42 specificity was much greater for experienced radiologists than that of less experienced
43 ones. Deep Learning and Data Science are widely employed in many fields of medical
44 imaging, and they have shown excellent results in Thoracic Imaging [12]. There have
45 been many approaches for diagnosing COVID-19 from CT and x-ray images that made
46 use of Deep Learning/Data Science recently.

47 There have been some efforts on using unsupervised learning based approaches for
48 this task. For instance, in [13], Mittal et al. developed an unsupervised learning-based
49 technique for COVID-19 diagnosis from multiple modalities of chest imaging. They used
50 a novel clustering based Gravitational Search algorithm for labelling the images into
51 covid and non-covid. They achieved an accuracy of 99.36% on the ultrasound dataset
52 but their approach achieved only 64.41% on CT dataset. In [14], Rui et al. used an
53 Pulmonary opacity detecting model trained using unsupervised learning over a small
54 dataset of COVID CT scan images and they achieved an accuracy of 95.5% for detection
55 of COVID-19.

56 A few object detection based approaches have also been used for detecting COVID-
57 19. For example, the authors in [15] proposed a YOLO based object detection model
58 for detecting and differentiating COVID-19 from other thoracic diseases. Their model
59 achieved a detection accuracy of 90.67%. In [16], Fatima et al. used single shot multi-box
60 detector based object detection technique which creates bounding boxes over the areas
61 of the chest x-rays and each bounding box is classified as normal or COVID-19. They
62 report an accuracy of 92% for classifying COVID-19.

63 The most used approach for solving this task has been using deep convolutional
64 neural networks (CNNs) with supervised learning [17–19]. As an example, a work
65 by Mukherjee et al. [20] proposed a deep CNN based architecture and trained it on a
66 combined data set of chest x-ray and CT images where they achieved an overall accuracy
67 of 96.28%. In [21], Li et al. proposed a stacked autoencoder model where the first four
68 layers consist of four autoencoders to extract better features from CT images. The final
69 model is built by chaining together these four autoencoders and linking them to the
70 dense layer and the softmax classifier. The authors report achieving an accuracy of
71 94.7% on the CT images data set. In [22], Chakraborty et al. proposed Corona-Nidaan, a
72 lightweight deep CNN architecture trained on chest x-ray data set with 3 classes which
73 achieved an accuracy of 95%. In [23], the authors used transfer learning with a VGG-16
74 model pre-trained on pneumonia detection and further fine tuned it over a COVID-19
75 detection data set achieving an accuracy of 93%, although they sometimes mis-classify
76 COVID-19, viral pneumonia, and normal cases. In [24], Khan et al. presented a Xception
77 network based architecture with pre-trained weights from ImageNet, which they fine
78 tuned over a 1.2K images data set and they report an overall accuracy of 89.5% on
79 multi-class classification. In [25], the authors proposed a two level pipeline with an
80 image segmentation block made up of a fully connected DenseNet backbone and a
81 classification block where Resnet-18 was used patch-wise which achieved an accuracy
82 of 91% upon training on a 354 images data set and upon evaluating over 99 images.
83 In [26], Mishra et al. presented an approach with a two neural network based system
84 and reported a maximum accuracy of 96%. Authors in [27] used an attention based

85 pre-trained VGG-16 model and fine tuned it over 3 data sets with 1125, 1638, and 2138
86 images, respectively. Upon evaluation, they achieved an accuracy of 79.58%, 85.43%,
87 87.49% over the three data sets, respectively. Shankar et al. [28] proposed a BMO-CRNN
88 algorithm for the covid-19 detection efficiently. In [29], Xueyu et al. fine-tuned multiple
89 pre-trained models over a 2500 CT scan images data set and achieved 82.5% accuracy.
90 Luz et al. [30] proposed models based on the EfficientNet family with a hierarchical
91 classifier and achieved an overall accuracy of 93.9%. Pham et al. [31] presented a
92 comprehensive study on transfer learning for COVID-19 detection from CT images by
93 training and comparing 16 pre-trained models.

94 After reviewing the relevant literature, it is clear that despite the effectiveness of deep
95 learning-based frameworks in COVID-19 identification, there are a few flaws. Most
96 of the models have been trained and evaluated on data sets with very less samples
97 which can lead to improper generalization due to which the model might perform very
98 poorly in real world and having a small test set might result in missing out on false
99 positives or negatives. With this motivation, we have conducted this research with main
100 contributions highlighted as follows:

- 101 • Due to lack of large public data sets, we collected and merged three standard
102 data sets ^{1,2,3} to form a 30K chest x-ray images COVID-19 data set for multi-class
103 classification and a 20K images data set for binary classification. These two data
104 sets have equal number of images in each class making it the largest and balanced
105 data set on COVID-19 imaging based detection available as open-source, which can
106 help the research community in training much more accurate and generalizable
107 models in the future.
- 108 • We implemented a model based on Vision Transformer (ViT) architecture on both
109 data sets and achieved a state-of-the-art overall accuracy of 98.4% in distinguishing
110 COVID-19 positive from normal x-rays, and an accuracy of 92.4% in distinguishing
111 COVID-19 from pneumonia and normal x-ray images.
- 112 • For evaluation, we fine-tuned multiple state-of-the-art baseline models which
113 are widely used in literature such as Inception-V3, Resnet-V2, EfficientNet-B0,
114 MobileNet-V2, VGG-16, Xception, and DenseNet-121 on both of the data sets and
115 compared these with our proposed model on multiple standard metrics.
- 116 • For better model interpretability and ease of diagnosis, we created Grad-CAM based
117 visualizations of COVID-19 progression in the lungs, which assists the diagnosis
118 process for healthcare.

119 The rest of this paper is divided into four sections, with multiple subsections within
120 each of them. Section 2 is focused on the proposed model's architecture and training
121 pipeline. Section 3 discusses the fine-grained details of our data collection and pre-
122 processing pipeline, followed by performance evaluation, comparison with baselines,
123 and interpretable visualizations. Section 4 presents an overview on the real-world utility
124 of our methodology in order to assist health services during emergency times. Section 5
125 concludes this work.

126 2. Model Architecture and Pipeline

127 This section covers information about the proposed transfer learning model as well
128 as critical parameter evaluations, fine-tuning steps, and model comparisons.

129 2.1. Architecture

130 After the success of Transformers in solving natural language processing problems
131 [32], Dosovitskiy et al. in [33] presented the Vision Transformer (ViT) model. When
132 trained on enough data, ViT beats state-of-the-art CNN with around four times less

¹ <https://data.mendeley.com/datasets/9xkhgts2s6>

² <https://data.mendeley.com/datasets/8h65ywd2jr/3>

³ <https://www.kaggle.com/endiqq/largest-covid19-dataset>

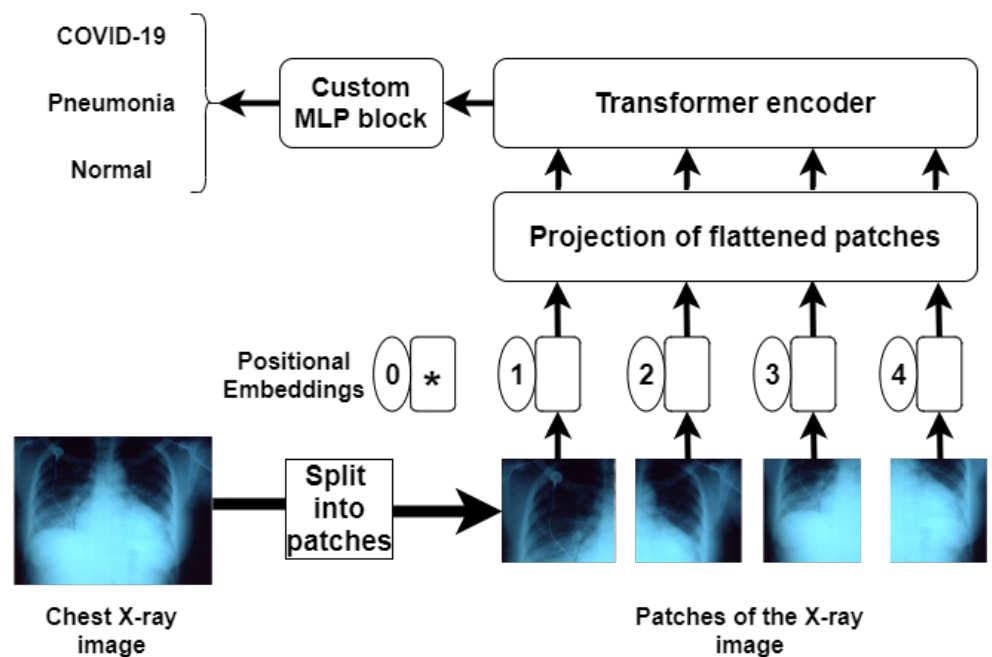


Figure 1. The proposed ViT model for COVID-19 detection.

133 computing resources. ViT tries to resemble the original transformer architecture [34]
 134 as much as possible. We designed a COVID-19 detection pipeline utilizing the Vision
 135 Transformer model and fine-tuned it on our dataset with a custom MLP block. The
 136 initial part of the network has a Patch Encoder layer which reshapes the input image into
 137 multiple flattened patches. Along with the patches, positional embeddings are added
 138 to form a sequence, because only sequential data is compatible with the Transformer
 139 encoders. The Transformer encoder used is same as [34] and contains multi-headed self-
 140 attention layers and multiple Multi-layer Perceptron (MLP) blocks. ViT's self-attention
 141 layer enables it to integrate information globally throughout the full picture. To recreate
 142 the visual structure from the training data, ViT learns to encode the relative placement
 143 of the patches. Self-attention has a quadratic cost as each pixel in the image is given as
 144 input, self-attention requires each pixel to pay attention to every other pixel. Because the
 145 quadratic cost of self-attention is prohibitively expensive and does not scale to a reason-
 146 able input size, the image is separated into patches. Because it does not establish any
 147 additional dependencies between the training images, Layer Norm is used before each
 148 block which assists in reducing training time and improving generalization performance.
 149 The overall architecture has been illustrated in Fig. 1.

150 2.2. Fine-tuning procedure

151 We used the ViT L-16 model for the initial stage of our model, which is the "Large"
 152 variant with a patch size of 16×16 . The ViT model had pre-trained weights from
 153 training on ImageNet data [35]. This initial stage consists of 23 transformer encoder
 154 layers stacked on top of each other. We removed the pre-trained MLP prediction block
 155 and attached an untrained set of feed-forward layers constituting the custom MLP block
 156 which can be seen in Fig. 2. The flattened output of the final transformer encoder is
 157 passed through two sets of batch normalization and dense layers constituting the MLP
 158 block. Batch normalization is a neural network layer that allows the model's other
 159 layers to learn more independently [36]. It is used to make the output of the preceding
 160 layers more natural and to make the activations scale the input layer. Learning becomes
 161 more efficient when batch normalization is utilized, and it may also be employed as a
 162 regularization to prevent model overfitting. The first dense layer consists of a Gaussian
 163 error linear unit (GELU) based activation with 120 neurons. GELU has been widely used

164 in revolutionary transformer models such as GPT-2 [37], BERT [38], and also in vision
 165 transformers [33] due to it's deterministic non-linearity that encapsulates a stochastic
 166 regularization effect [39], which leads to a major performance boost in most models with
 167 complex transformer architectures. The last dense layer has softmax activation and we
 168 use L2 regularization [40] to minimize overfitting as much as possible.

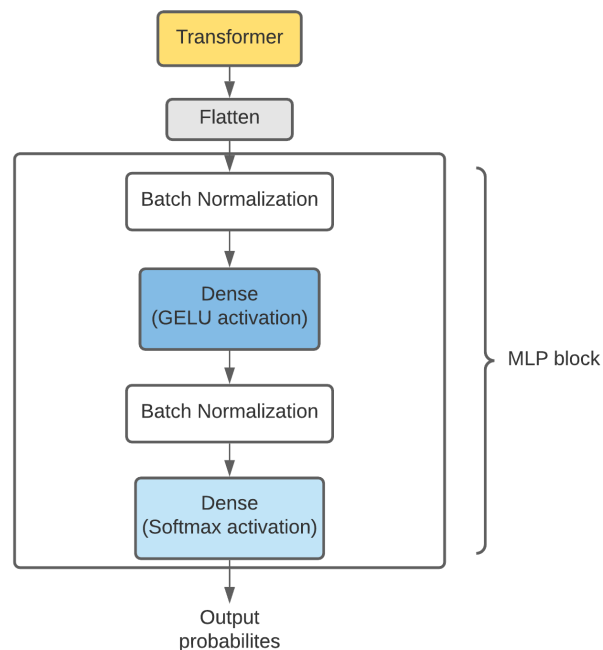


Figure 2. Custom MLP block attached to the Vision Transformer

169 2.3. Model training mechanism

170 We use the NovoGrad optimizer with a categorical cross-entropy loss function to
 171 train our model for multi-class classification, and binary cross-entropy loss in the case
 172 of binary classification. In each case, label smoothing of 0.3 was added which helps
 173 to make the neural network generalize on unseen data by adding noise to the labels
 174 [41]. NovoGrad performs similarly to SGD but with gradient normalization per layer,
 175 making the optimizer more robust to initial learning rate selection. When compared to
 176 Adam, NovoGrad uses less memory and is more numerically stable due to which the
 177 training time of our model reduced without a drop in performance. It broadens Adam
 178 and decouples weight decay from regularisation. It also has half the memory cost of
 179 Adam and similar memory needs to SGD with momentum. We also use the adaptive
 180 learning rate scheduler and callbacks from the Keras library [42] which automatically
 181 reduces the learning rate and stops over-training the model if the validation accuracy
 182 does not improve. The data set was randomly split into train/validation/test sets with
 183 75%/15%/10% of all the images, respectively.

184 As seen in Fig. 3, multiple metrics were monitored during the training process where all
 185 of those showed a progressively increasing curve even on validation.

- 186 **1. Accuracy:** The most common performance metric in any classification problem
 187 is the accuracy metric. For the multi-class classification, the categorical accuracy
 188 was chosen which resembles the average accuracy over all the three classes of chest
 189 x-ray images. The binary classification involved the binary accuracy metric which
 190 measures how many times the predicted label matches the true label for the chest
 191 x-ray image.

192

- 193 2. **AUC score:** The area under the ROC curve (AUC) score shows how well predic-
194 tions are ranked across all the classes and how much the model can distinguish
195 between each class. It ensures that performance across all feasible categorization
196 criteria is aggregated. It has been proved in the literature that AUC score is a more
197 robust metric to measure the ability of a classifier than the accuracy [43].
198
- 199 3. **Precision:** Precision is defined as the number of true positives divided by the
200 number of true positives plus the number of false positives.
201
- 202 4. **Recall:** Recall is defined as the number of true positives divided by the number of
203 true positives plus the number of false negatives.

204 3. Experimental Results and Discussion

205 3.1. Data set

206 We constructed a three-class data set of 30K chest x-ray pictures with labels COVID-
207 19 - for patients with COVID-19 infection; normal - for stable patients; and pneumonia -
208 for patients with viral and bacterial pneumonia, following the pattern of likely classes
209 reported in the literature. We took 5500 COVID images and 4044 normal images from
210 El-Shafai et al. [44]. Another 1281 COVID-19 images, 3270 normal images, and 4657
211 pneumonia images were taken from Sait et al. [45]. Finally, we took 3000 normal images,
212 6045 pneumonia images, and 4038 COVID-19 images from the COVID-Ti data set by Qi
213 et al. [46]. The distribution of the aggregated data has been visually illustrated in Fig. 4.
214 To make our data set completely balanced we sampled top 10K images from each class
215 by ranking them based on resolution, making it a chest x-ray data set of 30K images
216 for COVID-19 detection. This is, to the best of our knowledge, the largest open source
217 collection of chest x-ray images for the detection of COVID-19 and pneumonia till date.

218 3.2. Pre-processing

219 Each image in the gathered data set is passed through a minimal image pre-
220 processing pipeline which ensures to make all images compatible for the model training.
221 The following are the steps in the pipeline:

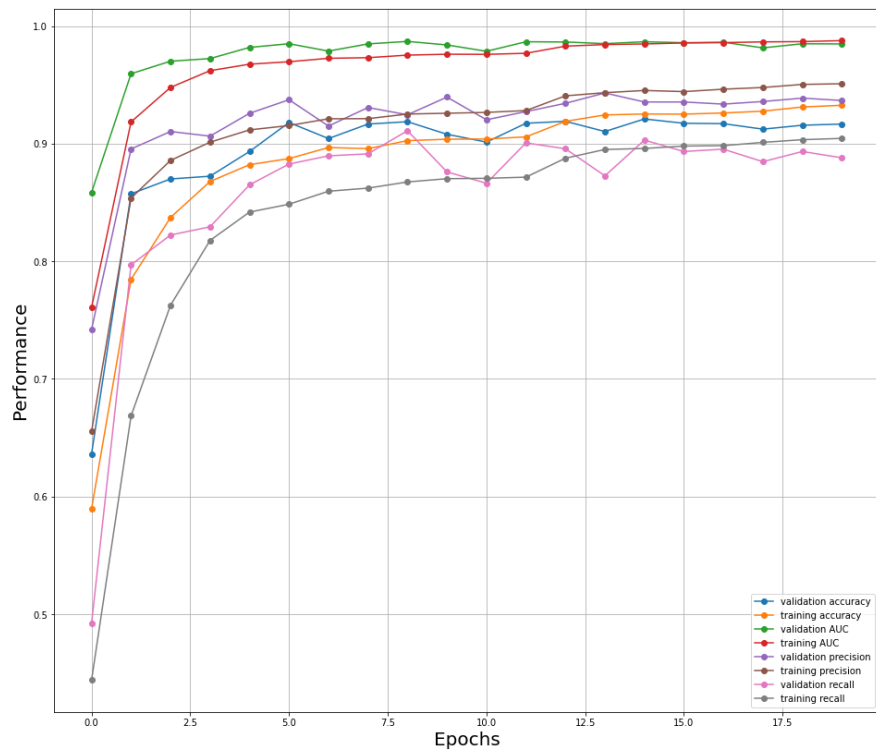
- 222 1. **Resize:** As neural network models have a fixed-size input layer, all images must
223 be scaled to the same size. Therefore, we resize all the images in the data set to 224
224 $\times 224$ pixels.
225
- 226 2. **Interpolation:** There are a few images in the data set which are of size lesser than
227 224×224 . While increasing their size, the estimation of new pixels needs to be
228 done efficiently in order to retain quality. This process is termed "Interpolation" of
229 images. For our pipeline we used the nearest neighbour interpolation, in which
230 the closest pixel value to the supplied input coordinates is used to approximate the
231 output pixel value. This approach is straightforward to implement, and there is no
232 bogus data in the end result [47].

233 3.3. Data augmentation

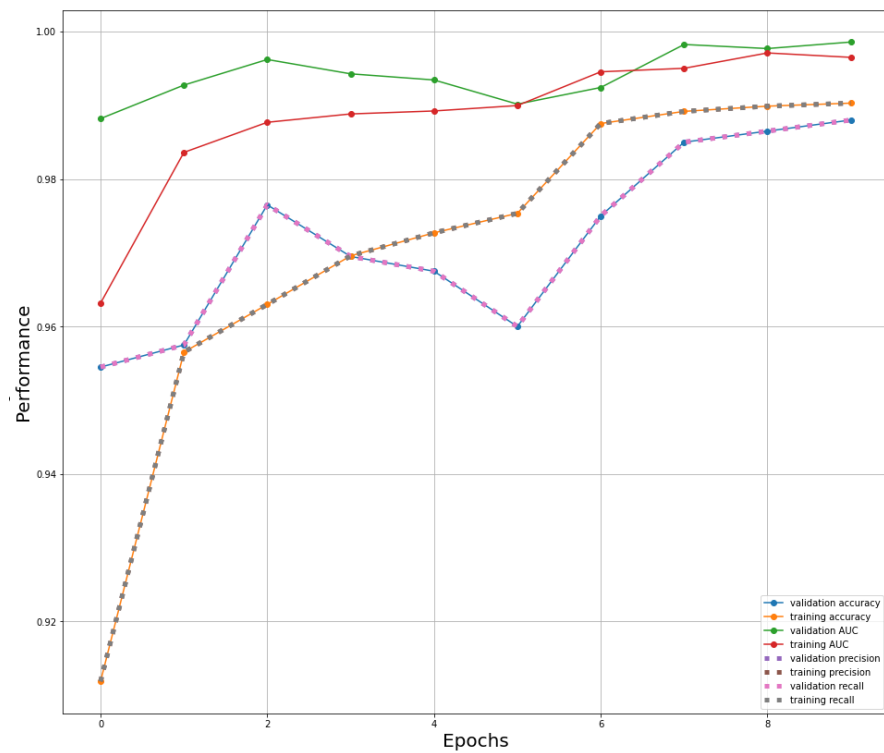
234 In order to develop accurate and generalizable deep learning models, supervised
235 learning requires large amounts of data. In our training pipeline, we employed a variety
236 of data augmentation techniques such as random rotation, width shift, height shifts, and
237 flipping which have been demonstrated in the literature to be beneficial in increasing
238 deep learning model performance [48,49].

239 3.4. Testing environment

240 All the training and testing pipelines for the proposed models, as well as baselines
241 were implemented using TensorFlow 2.4 framework [50] in a Python 3.8 virtual environ-
242 ment. The graphics processing unit used in the training pipeline was a 4.1 TFLOPS Tesla



(a) Multi-class performance analysis



(b) Binary-class performance analysis

Figure 3. Performance measures during training

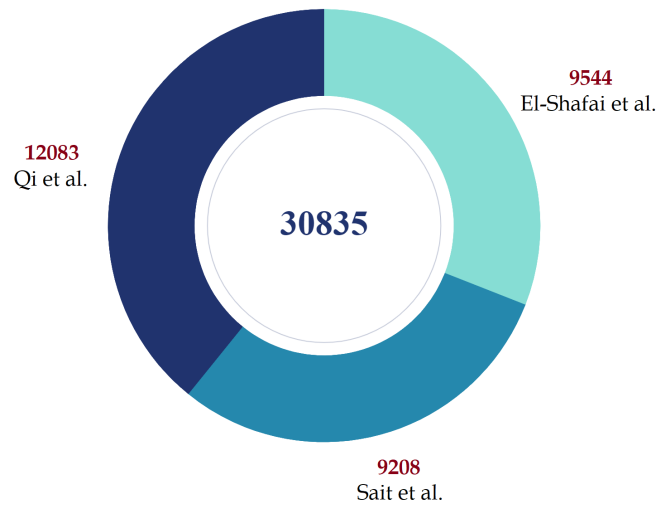


Figure 4. Data set distribution and description

243 K80. The net available RAM was 24 GB. Jupyter notebooks were utilized to conduct the
244 experiments.

245 3.5. Model evaluation

246 Our proposed COVID-Transformer was evaluated over the test set of both of our
247 multi-class and binary classification data sets. It can be observed from Fig. 5(a) that our
248 model is capable in distinguishing between all the three classes very accurately. Although
249 the amount of false positives and true negatives are less, but the model sometimes
250 confuses between COVID-19 and other types of pneumonia, which is acceptable as
251 COVID-19 is itself a form of pneumonia and it is very tough even for expert radiologists
252 to distinguish between the two. As observed in Fig. 5(b), our proposed model performs
253 extremely well over the binary classification data set with only 21 out of 1000 images
254 misclassified. The overall performance metrics over the test data sets have been outlined
255 in Table 1. The multi-class classification model works well, with an accuracy of 92% and
256 an AUC score of 98%. In this situation, the accuracy is lower than the AUC score because
257 only images projected as pneumonia but really COVID-19 are misclassified, while all
258 other categories are correctly classified, hence the AUC score is not much affected. The
259 binary classification model achieves an accuracy of 98% and an AUC score of 99% which
260 is suitable for real-world deployment as a diagnosis tool for detecting COVID-19 as it
261 has significantly higher performance than standard RT-PCR tests.

262 3.6. Ablation experiments

263 In order to ensure that our transfer learning architecture is optimal, we conduct
264 a comprehensive ablation study on the multi-class classification data set. We first
265 experiment by modifying the custom block using different number of layers, activations,
266 and order of layers. First, we observe that using only one dense layer with Batch
267 normalization and ReLU activation, the accuracy drops down to 90%. Upon removing
268 the Batch normalization the accuracy further degrades to 89%. However, if we replace
269 ReLU with the GeLU activation function, a single dense layer with Batch normalization
270 achieves an accuracy of 91% and 90% without Batch normalization. This shows that
271 GeLU activation is slightly more effective in processing the outputs of the stacked
272 transformer encoders compared to the ReLU activation. Next, we further experiment
273 with a custom MLP block of two GeLU activated dense layers with and without batch
274 normalization, where the accuracy increases to 92% and 91%, respectively. However, if
275 we further add another dense layer with and without batch normalization, the training

Model	Accuracy	Precision	Recall	F1 score	AUC
Binary-class	0.98	0.97	0.97	0.97	0.99
Multi-class	0.92	0.93	0.89	0.91	0.98

Table 1: Evaluation of the proposed model

276 accuracy increases whereas the testing accuracy drops to 88% and 89%, respectively.
 277 This is a clear indication that our model results in overfitting beyond 2 dense layers, thus
 278 we decide to keep a custom MLP block with two batch normalization and dense layers
 279 in the final architecture.

280 3.7. Comparison with baseline models

281 As our data set has not been evaluated using other models in the literature, we fine-
 282 tuned some of the widely used state-of-the-art models on both variants of our data set.
 283 All the data preparation and image augmentation steps are same for the baselines, except
 284 for some of the pre-processing functions which are necessary for input to the models.
 285 For Inception-V3 and Xception fine-tuning, the images were re-sized to 299×299 pixels.
 286 The same data augmentation techniques as for our proposed COVID-Transformer model
 287 were used. The MobileNet-V2, ResNet-V2-50, DenseNet-121, VGG-16, and EfficientNet-
 288 B0 models have a standard size requirement of 224×224 pixels, which is same as
 289 of our COVID-Transformer model, thus we used the same data pre-processing and
 290 augmentation steps for fine-tuning them. From Table 2, it can be noted that among
 291 the baselines, MobileNet-V3 and Xception perform the best with 90% Accuracy on the
 292 multi-class classification problem. Our COVID-Transformer model outperforms all the
 293 baselines in terms of accuracy, precision, F1 score, and AUC score.

294 3.8. Grad-CAM visualization

295 For better visual representation and model interpretability, the Grad CAM Map
 296 based illustration introduced by Selvaraju et al. [51]. is shown in Fig. 6. The Grad
 297 CAM Map visualization has the capability to highlight affected areas of the lungs that
 298 are significant for disease predictions as well as disease development. The images are
 299 obtained by passing the output of the embedding layer present in our model at the
 300 beginning just after the input layer.

301 Fig. 6(a) shows a normal patient with no disease having no highlighted region in
 302 the lungs. Fig. 6(b) shows pneumonia patient's lungs with affected regions highlighted
 303 in blue and green. Fig. 6(c) shows a COVID-19 infected patient with mostly yellow and
 304 red highlighted regions which indicate severe infection. The figure clearly shows that
 305 our suggested methodology recognizes and differentiates relevant impacted areas from
 306 COVID-19 and other pneumonia images. COVID-19 impacts the lungs considerably
 307 more intensively than other types of pneumonia, hence our model emphasises this by
 308 highlighting yellow and red areas in the COVID patient's x-ray image.

309 4. Case Study in Medical Services

310 Health systems in both rich and poor nations were overburdened by the COVID-19
 311 outbreak. Sustainable Development Goals (SDGs) planned for 2025 will be affected by
 312 the pandemic-related losses, there is no question about it. As a result of the epidemic,
 313 there was a window of opportunity to take use of current digital solutions and discover
 314 new ones. These solutions can aid in the fulfilment of the SDGs, particularly those
 315 that pertain to health. In this sense, achieving global health coverage is an important

Model	Accuracy	Precision	Recall	F1 score	AUC
Inception-V3 [31]	0.90	0.89	0.91	0.89	0.92
EfficientNet-B0 [30]	0.89	0.88	0.89	0.88	0.92
MobileNet-V2 [31]	0.90	0.90	0.89	0.90	0.92
ResNet-V2 [29,31]	0.88	0.87	0.86	0.86	0.93
VGG-16 [23,27,29,31]	0.87	0.87	0.85	0.86	0.90
Xception [24,31]	0.90	0.92	0.87	0.90	0.93
DenseNet-121 [25,29,31]	0.88	0.90	0.85	0.87	0.92
COVID-Transformer (Ours)	0.92	0.93	0.89	0.91	0.98

Table 2: Performance comparison of our COVID-Transformer with baseline models on the multi-class classification problem

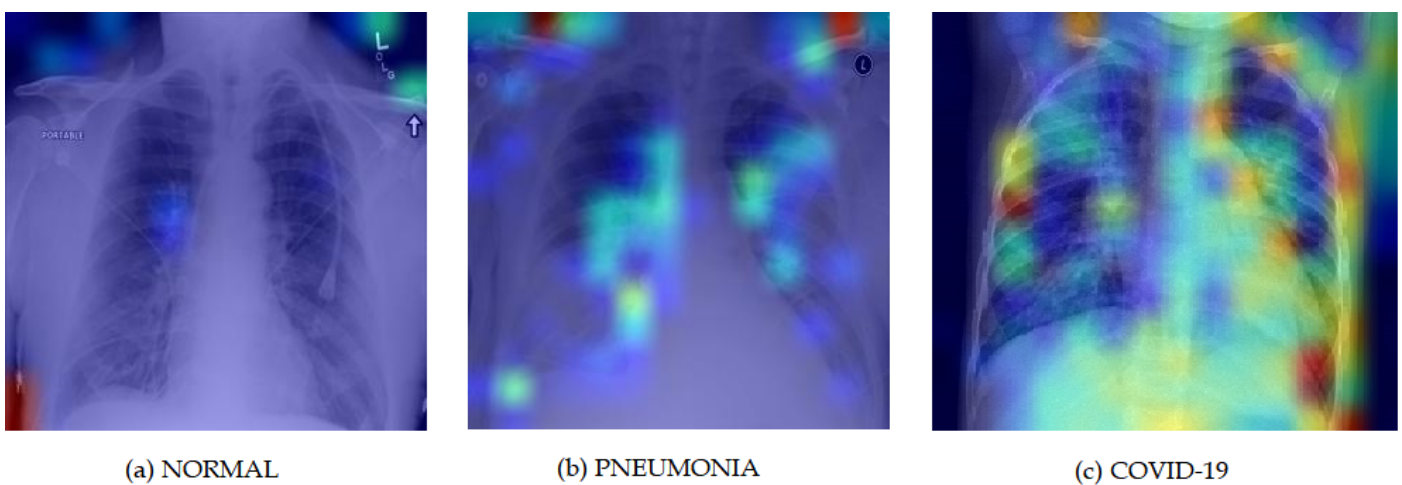


Figure 6. Grad-CAM visualization for the three classes

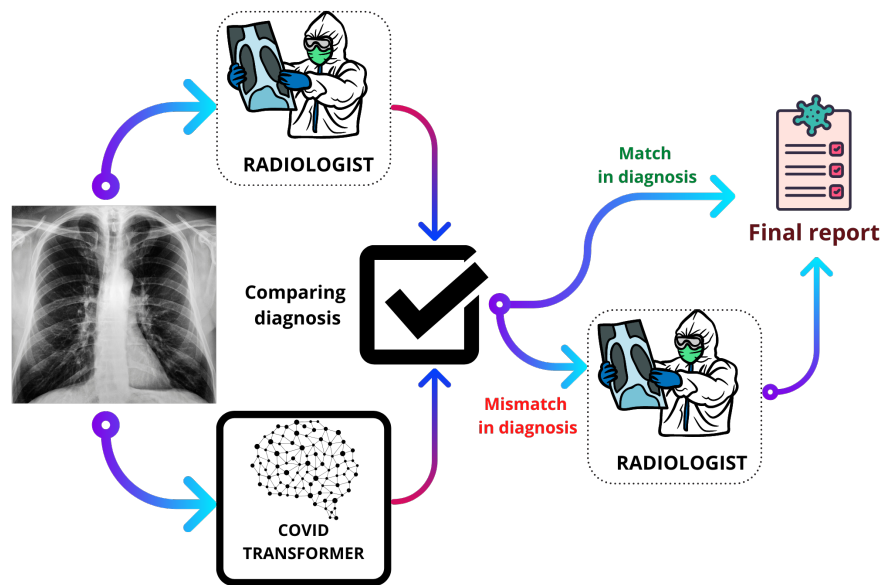


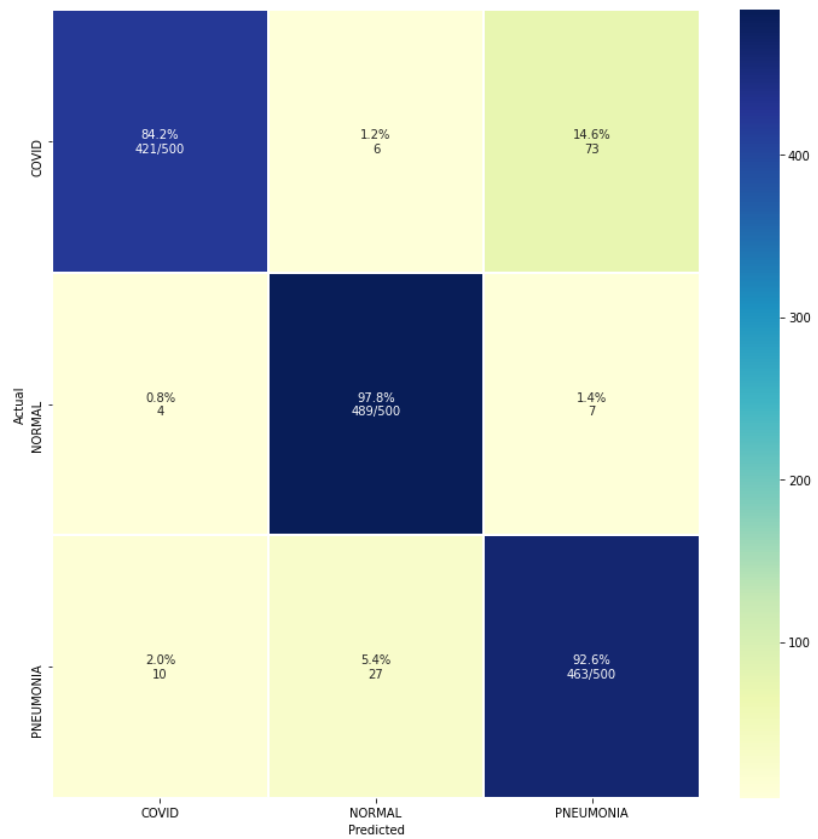
Figure 7. Flow of deployable solution

316 SDG. Early-diagnosis is an important factor in reducing the number of deaths from
 317 COVID-19, which almost becomes impossible when there is a steep rise in infections
 318 concentrated in a particular location. If an infected individual is isolated at the right time,
 319 multiple infections from further transmissions can be prevented. Our proposed method
 320 for X-Ray based detection of COVID-19 would be an efficient addition to the healthcare
 321 system boosting the global health coverage. It can be used as an aid for radiologists
 322 to reduce human-errors in their diagnosis, as well as can be used as a single tool to
 323 detect COVID-19 in places where radiologists are not adequate due to infections rising
 324 at a breakneck pace. Fig. 7 shows the typical flow of our method when deployed in a
 325 real-world setting to have zero human-error diagnosis.

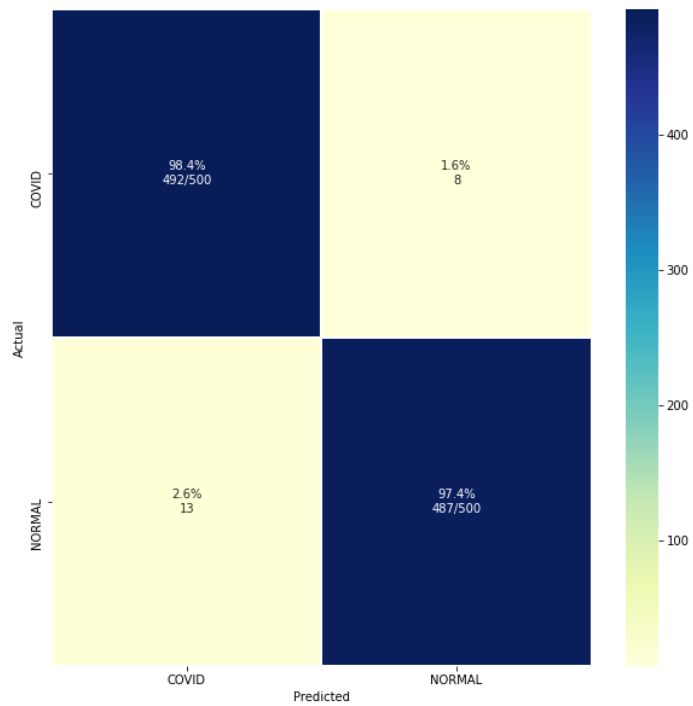
326 5. Conclusion

327 In this research, we proposed a robust and interpretable deep learning model
 328 that can efficiently diagnose COVID-19 infection at scale in real-world situations for
 329 healthcare. For this objective, a 30K chest x-ray image collection was produced by
 330 combining several open-source data sets. The model architecture chosen was based on
 331 the Vision Transformer and it showed high performance with accuracy and AUC score
 332 as high as 98% and 99%, respectively. For making our model trustworthy, we made an
 333 interpretable inference pipeline with Grad-CAM based visualizations per image. We
 334 believe that with the help of our proposed approach, chest x-ray images can also be
 335 used as a crude and low-cost bed-side diagnostic tool for detecting COVID-19. This may
 336 be extremely valuable in areas where quick testing is unavailable, and it may also be
 337 used as a second screening method after the standard RT-PCR test to verify that any true
 338 negative or false positive cases do not occur. Our future work will focus on proposing
 339 another variant of the Vision Transformer for further improving the performance, given
 340 the availability of larger data sets.

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 342 contributed to the concept and methodological parts. D. Shome did the experimental analysis along
 343 with T. Kar, S.N. Mohanty, and P.Tiwari. K. Muhammad and Y. Zhang assisted in experiments and
 344 also provided the feedback. S.N. Mohanty, P.Tiwari, K. Muhammad, Abdullah AlTameem, and



(a) Multi-class confusion matrix



(b) Binary-class confusion matrix

Figure 5. Confusion matrix for both types of classification

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